

Fig.1 Sample images from the benchmark database

The CA, TA and CD are extracted for each region in the image and the extracted features are combined into a single vector for each region in the image and are normalized as aforementioned in section 2.4. The similarity measure is computed for the feature vector of corresponding regions of both query and target images then the average result of the similarity measure of all the regions of an image is considered for final result.

Different sub-sets of query images from the entire benchmark database is selected to assess the performance of the proposed system and number of images in each sub set is differing depends on the number of images in each modality category. The experiments are executed in the dual core processor, 2 GB memory and 64 bit windows operating system and are carried out using the MATLAB.

*B. Performance assessment*

To assess the performance of the proposed system, we used average retrieval precision (MAP) [23]. Let  $I_N$  be the first N number of images retrieved akin to the query image, M be the number of images in the benchmark database akin to query image, then precision and recall calculation is done as follows in equations (6) and (7) respectively.

$$\text{Precision (P)} = \frac{I_N}{N} \tag{6}$$

$$\text{Recall (R)} = \frac{I_N}{M} \tag{7}$$

For instance the values of  $I_N$ , N and M are 60, 100 and 592 respectively then precision  $P(100)$  is  $60/100=60\%$  and recall  $R(100)=60/592=0.10\%$ . The average precision versus recall for CT, MRI, Mammogram, Ultrasound, X-ray images in the proposed and existing system [11] is shown in Fig.2. We also incorporated G-measure which combined the results of precision and recall into single result and provides better results [23] and is computed as follows in equation (8). In Table 2, the G-measure for CT, MRI, Mammogram, Ultrasound and x-ray images are reported.

$$GM = \sqrt{\text{Precision} \times \text{Recall}} \tag{8}$$

It is observed in the results that the proposed combination CA, TA and CD features significantly outperforms the method in [11] and it is because of capturing of local spatial correlation of identified texture elements; capturing the

geometric features of prominent edges. The average precision Vs recall of the proposed work and existing work for different modalities

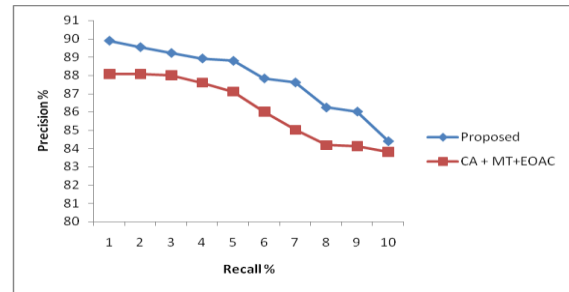


Fig. 2 CT

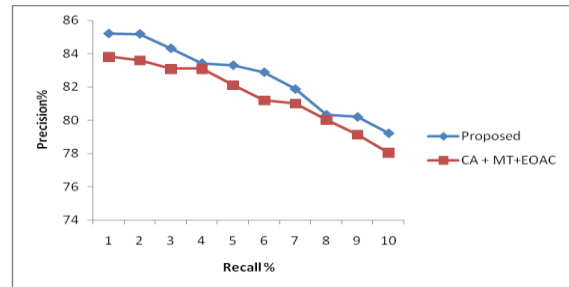


Fig. 3 MRI

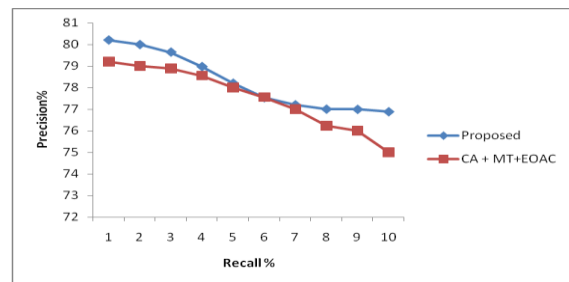


Fig. 4 Mammogram

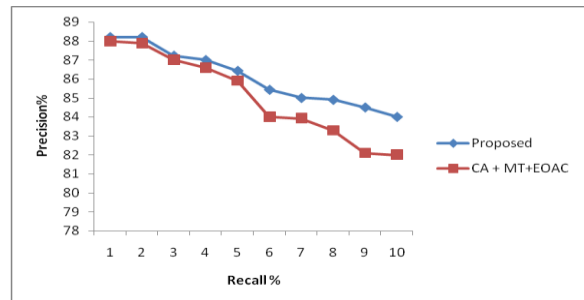


Fig. 5 Ultrasound

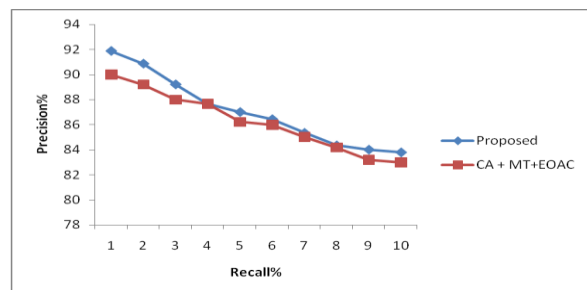


Fig. 6 X-ray

TABLE I GM FOR THE PROPOSED AND EXISTING SYSTEMS FOR THE IMAGES OF VARIOUS MODALITIES IN THE BENCHMARK DATABASE

Method	CT	MRI	Mammogram	Ultrasound	X-Ray
Proposed	87.85	82.61	78.27	86.09	87.05
Existing	86.20	81.56	77.54	85.07	86.25

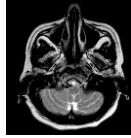


Fig. 7 Example query image

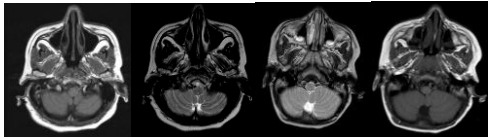


Fig. 8 Top 4 retrieval results obtained with the proposed system corresponding to the query image

#### IV. CONCLUSION

In this paper, we have proposed a hybrid framework for fast and efficient medical image retrieval system using color autocorrelogram, texture autocorreloram and chordigram features. The proposed combination of features is very effective in representing color, texture and shape features. Moreover, features are extracted for each non-overlapping rectangular regions of the image and the similarity measure is computed for the corresponding regions of both query and target images then the average result of the similarity measure of all the regions in the image is considered for final result which also leads to significant increase in the accuracy. The accuracy of the proposed system is significantly better than that of the existing system and it will be very useful for people working in the medicine domain.

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